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64 Method and apparatus for displaying a single parameter image

⑦ A method and apparatus for displaying an image which has a wide dynamic range. Low spatial frequency components $f(x,y)$ of the image are extracted from the image signal and are presented as a color overlay which tints an intensity modulated display of local high spatial frequency image components $a(x,y)$.

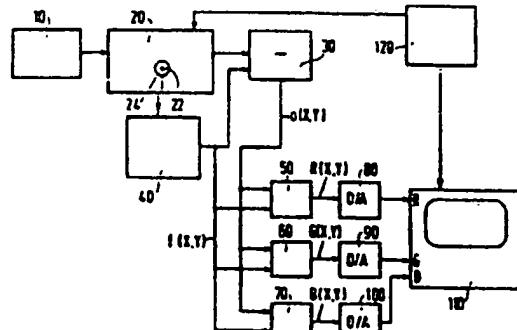


FIG. 2

EP 0 213 666 A1

Method and apparatus for displaying a single parameter image.

The invention relates to a method for displaying an image from an image signal which includes values of a parameter at a large number of image points and which has a wide dynamic range, comprising the steps of filtering the 5 image signal to extract, at each image point, a low spatial frequency background signal component and a rapidly varying local signal component and compressing the dynamic range of the local signal component.

The invention also relates to an apparatus for 10 displaying an image comprising:

means which produce an image signal which includes parameter values at a large number of image points and which has a wide dynamic range;

filter means which extract a low spatial frequency, 15 background component of the image signal;

display means which map each image point into a corresponding pixel on an image display; and

means which modulate the intensity of each pixel to represent the high spatial frequency components of the 20 image signal at the corresponding image point.

The invention is particularly useful for displaying medical diagnostic images which are produced, for example, by echo ultrasound or other digital imaging modalities.

Under ideal conditions, the human visual system is only able 25 to perceive from four to six bits of dynamic range (from 16 to 64 distinct gray levels) in a monochrome image. The actual number of bits perceived is further reduced in the presence of additive glare (background lights) which usually means that a darkened room is required for presentation of images 30 with a large dynamic range. The perceived dynamic range of an image may be increased by reducing the amplitude of lower spatial frequencies, but this dynamic range reduction is

detrimental to effective diagnosis of medical images, particularly ultrasound images, which makes use of the presence of shadowing and/or bright-up.

Many algorithms for compressing the dynamic range of a one-dimensional image exist in the prior art. For example, homomorphic filtering which can emphasize local high frequency variations in an image while suppressing low spatial frequency variations is described in Oppenheim, Schaffer and Stockham, "Nonlinear Filtering of Multiplied and Convolved Signals", Proceedings of the IEEE, Vol. 56, pages 1264-1291 (1968) and in "Digital Image Restoration", Andrews and Hunt, Prentice-Hall Inc., 1977, which are incorporated herein, by reference, as background information. In one such technique, the average value of pixels in the local two-dimensional region surrounding each pixel is computed and is divided into the value of the individual pixel. The quotient represents the local, high frequency variation and is used to intensity modulate the display of the pixel. This results in a compression, similar to AGC compression of audio signals. However, these techniques generally "throw-away" the low spatial frequency, background information from the image.

It is an object of the invention to provide a method and an apparatus for producing images that combine the features of an extended perceived dynamic range and a good display of low spatial frequency information.

To achieve this object the method according to the invention is characterized in that it further comprises the steps of displaying each image point by modulating the intensity of a corresponding image pixel to represent the compressed local signal component at the image point and modulating the color of the pixel to represent the background signal component.

The apparatus according to the invention is characterized in that it further comprises color modulating means for modulating the color of each pixel to represent the background component of the image signal at the corresponding image point.

In accordance with the invention, low frequency background information is displayed as a color tint which overlays an intensity modulated display of a high spatial frequency, compressed image. The invention thus converts 5 low frequency information, which is normally discarded by compression, into another form which the observers can simultaneously perceive in conjunction with the compressed, high frequency image.

The invention will now be described in detail by 10 reference to the attached drawings in which:

Figure 1 is a simplified chromaticity diagram which illustrates the invention;

Figure 2 is an image display system which incorporates the invention; and

15 Figure 3 are plots of RGB multiplier values.

It is well known that pseudocolor enhances human perception of gray scales and enables an observer to quantify a single parameter image. It has also been shown that color can allow the eye-brain combination to form useful 20 correlations on multidimensional image data, if it can be used in a pleasing manner. However, many medical radiologists do not like pseudocolor images.

It is known that separate use of red, green and blue to image three independent variables leads to confusing 25 images. A more natural presentation is used in commercial color television and in map making where a primary image is shown as a high (spatial) resolution intensity image and secondary parameters are visualized by color tinting (which typically has less spatial resolution than the 30 primary image). Thus, the hue (color) and the saturation (purity of color) can be used to present two independent low-resolution variables which are superimposed on a high resolution intensity image.

Figure 1 schematically illustrates a two-dimensional 35 chromaticity space of hue H and saturation S in polar coordinates. In the figure, $S = 0$ is white (zero color saturation) and the circle $S = 1$ represents pure mono-

chromatic colors (fully saturated) such as blue (B), yellow (Y), red (R) and violet (V). In this model, locations near $S = 0$ are pastel colours such as pink (P) and skyblue (SB).

6 In the prior art, three parameters of position in an image (such as $a(x,y)$, $f(x,y)$ and $g(x,y)$ were respectively assigned to Intensity, Hue and Saturation as, for example:

$$\text{Intensity : } I(x,y) = K_i a(x,y) \quad (1)$$

$$10 \quad \text{Hue : } H(x,y) = K_h f(x,y) \quad (2)$$

$$\text{Saturation: } S(x,y) = K_s g(x,y) \quad (3)$$

where K_i , K_h , and K_s are constants.

15 The simplest use of these relations is to set $S = 0$ (which implies that the hue is irrelevant). Black and white intensity images are thus produced from the function $a(x,y)$.

20 In the usual prior art pseudocolor display, the parameter, $I(x,y)$ is a constant, S is unity (fully saturated color), and the parameter $f(x,y)$ is imaged with hue as the only variable. Many people find such images distasteful.

25 In a more acceptable prior art method, "color tinting" of a gray scale image is accomplished using all three equations. If two parameters are of interest, it is common to set S equal to a constant and to use $I(x,y)$ and $H(x,y)$ as the parametric variables. Color tinting of a black and white image usually conveys low resolution information as an overlay through which the observer can see an image of intensity information $a(x,y)$ in the same 30 manner as a color tinted black and white photograph.

If S is chosen as unity, this scheme is still unsatisfying to many observers. More pleasing images are formed if S is set to a small value which presents all colors as unsaturated pastels.

35 My copending patent application No. (PHA.21,278) discloses a method and apparatus for simultaneously displaying two parameters in an image which can advantageously

be utilized with the present invention. A combination of hue and saturation coding is used to overlay a display of a secondary parameter display on an intensity modulated display of a primary parameter.

5 In accordance with that invention, a second parameter $f(x,y)$ is used to tint an intensity image $I(x,y) = a(x,y)$ by controlling a combination of hue $H(x,y)$ and saturation $S(x,y)$ at each pixel so that the hue of the pixel is determined by the sign of the deviation of the 10 value of the second parameter from a reference value, f_0 , and the saturation of the pixel is proportional to the absolute value of that deviation. For example:

when $f(x,y) \leq f_0 : H(x,y) = \text{Blue}$

15
$$S(x,y) = C_1 \frac{f_0 - f(x,y)}{(f_0 - f_{\min})}$$

and when $f(x,y) > f_0 : H(x,y) = \text{Red}$

20
$$S(x,y) = C_1 \frac{f(x,y) - f_0}{(f_{\max} - f_0)}$$

where C_1 , f_{\max} , f_{\min} , and f_0 are constants. Thus, as f increases from its minimum to its maximum, the chromaticity follows a path, as illustrated by the broken arrow A in 25 Figure 1, from a relatively saturated blue B through the pastel shades of blue SB through white ($S=0$) and then through a pastel P and into a relatively saturated red color R. Any radial path inward from a saturated color to white and out again along another radial path to some contrasting 30 color may be used. In a preferred embodiment, the path begins and ends at somewhat unsaturated pastel colors as this seems to provide a more pleasing image.

In a preferred embodiment of the present invention, the low frequency background variation of a compressed 35 image is used as a secondary parameter to modulate the hue and saturation of the pixels so that, for example, shadow areas of the image are displayed as ice blue, average density regions of the image are displayed as shades of

gray and highlights of the image are displayed with an intense red overlay.

The principle features of the displayed image are:

- 5 1) when the low frequency component does not deviate from its reference or equilibrium value, then the image is black and white without color tint; and
- 10 2) the color overlay has a linear (one dimensional) directional sense (for example: from blue to red) which may be mentally associated as left-right, up-down, hot-cold, good-bad, big-little, etc. In contrast, conventional hue modulation along has "circular loop" connotations which can sometimes be disorienting.

Figure 2 is a block diagram of an image display system which incorporates the invention. A scanner 10 produces a stream of digital data wherein each word represents the value of an imaged parameter at a discrete point in an image matrix. The scanner 10 may, for example, be an echo ultrasound scanner, an X-ray computed tomography scanner, a magnetic resonance imaging device, a digital subtraction radiography system, or a similar medical imaging device. Alternately, the scanner 10 could represent the output of an electron microscope, a computer graphics unit, or a radar system. At the output of the scanner 10, the data which represents points in the image can each assume more than from 16 to 64 discrete values and each word is therefore represented by more than from 4 to 6 bits. Typically, each image point will be represented by from 8 to 32 bits. Data from the output of the scanner 10 is stored in an image memory 20. The image memory contains a discrete, addressable memory cell for each point in the image.

The contents of the image memory 20 are scanned, by addressing the memory on an image point-by-image point basis and the successive values at image points 22 in the image matrix are fed to a first input of a digital dividing circuit 30. At the same time, the values of all image points

in a local area 24 of the matrix, which surrounds the addressed image point 22, are fed to an average value computing circuit 40. The average value of the image points in the area 24 is a measure of the low spatial frequency 5 background components $f(x,y)$ at the addressed image point 22. The high order bits from the output of the average value circuit 40 are fed to a second input of divider circuit 30.

The average value circuit 40 and divider circuit 30 function as a two-dimensional, homomorphic low-pass filter 10 which extracts a slowly varying background component from the image signal. Alternately, other known types of low-pass filters may be utilized. In some applications it is also possible to extract the background component of the image signal using a one-dimensional filter. For example, the 15 background component can be extracted from echo-ultrasound or radar signals with a one-dimensional low-pass filter which operates on the logarithm of the A-line signals in the time domain.

Alternately, if the image signal is subjected to 20 logarithmic compression before it is stored in the image memory, a subtraction circuit can be utilized in place of the divider circuit 30.

The divider circuit 30 divides the first input, which is the value of image point 22, by the low frequency 25 component $f(x,y)$ to yield a function $a(x,y)$ which represents the high spatial frequency, low order bit variation at image point 22. The high order bits of the low spatial frequency component, $f(x,y)$, and the low order bit of the high spatial frequency component, $a(x,y)$ are combined and 30 used to address the respective contents of three read-only memories (ROM's) 50, 60 and 70. Read-only memories 50, 60 and 70 respectively contain look-up tables which determine, from the values of the functions $f(x,y)$ and $a(x,y)$ the values of the red, green, and blue components of a 35 corresponding pixel in a display of the image. The outputs of read-only memories 50, 60, and 70 are fed, respectively, through digital-to-analog converters 80, 90 and 100 to the

red, green, and blue inputs R, G, B of an RGB CRT display 110. A sweep control circuit 120 generates horizontal and vertical sweep signals to produce a raster scan on the display 110 and to simultaneously address the scan-in image memory 20, so that the image memory cells 22 in the image memory 20 are mapped to corresponding pixels on the face of the CRT in the display 110.

In preferred embodiment of the invention, the look-up tables in the ROM memories 50, 60, and 70, respectively generate a red signal, $R(x,y)$, a green signal $G(x,y)$, and a blue signal $B(x,y)$ in accordance with the formulas

$$\begin{aligned} I(x,y) &= K_i a(x,y) \\ R(x,y) &= P_R(x,y) I(x,y) \\ 15 \quad G(x,y) &= P_G(x,y) I(x,y) \\ B(x,y) &= P_B(x,y) I(x,y) \end{aligned}$$

where the multiplier values P_R , P_G and P_B are all less than unity and are functions of $f(x,y)$ determined according to the mapping illustrated by the straight lines in Figure 3. 20 When P_{min} differs from zero, maximum saturation is not obtained. When the output of the average value circuit 40 is equal to the nominal value of the image intensity, f_0 , all three color guns are balanced to produce a nominally white pixel. In that case $P_R = P_G = P_B = P_w$. 25 It is also possible to obtain a particularly pleasing modulation schema by varying the value of P_w . That is to say the value of the intensity ($I = R+G+B$) is in fact slightly modulated by $f(x,y)$.

CLAIMS

1. A method for displaying an image from an image signal which includes values of a parameter at a large number of image points and which has a wide dynamic range, comprising the steps of filtering the image signal to extract, at each image point, a low spatial frequency background signal component and a rapidly varying local signal component and compressing the dynamic range of the local signal component, characterized in that the method further comprises the steps of displaying each image point by modulating the intensity of a corresponding image pixel to represent the compressed local signal component at the image point and modulating the color of the pixel to represent the background signal component.
2. A method as claimed in Claim 1, characterized in that the filtering step comprises filtering the image signal with a low-pass filter.
3. A method as claimed in Claim 2, characterized in that the filtering step comprises filtering the image signal with a two-dimensional low-pass filter.
4. A method as claimed in Claim 2 or 3, characterized in that the low-pass filter is a homomorphic filter.
5. A method as claimed in any one of Claims 1-4, characterized in that the step of modulating the color of the pixel comprises displaying the background signal by modulating the hue of the corresponding pixel to a first color when the background signal is greater than a predetermined reference value, modulating the hue of said pixel to a second, complementary color when the background signal is less than the reference value and modulating the saturation of the color of the pixel in proportion to the absolute value of the deviation of the background signal from the reference value.

6. A method as claimed in Claim 5, characterized in that the first color is red and the second color is blue.

7. A method as claimed in any one of Claims 1-6, characterized in that the image signal represents a medical diagnostic image.

8. Apparatus for displaying an image comprising: means which produce an image signal which includes parameter values at a large number of image points and which has a wide dynamic range;

9. filter means which extract a low spatial frequency, background component of the image signal;

display means which map each image point into a corresponding pixel on an image display; and

10. means which modulate the intensity of each pixel to represent the high spatial frequency components of the image signal at the corresponding image point; characterized in that the apparatus further comprises:

11. color modulating means for modulating the color of each pixel to represent the background component of the image signal at the corresponding image point.

9. An apparatus as claimed in Claim 8, characterized in that the color modulating means are designed to display the low frequency, background component by modulating the hue of the corresponding pixel to a first color when the 12. background component is greater than a predetermined reference value, modulating the hue of said pixel to a second, complementary color when the background component is less than the reference value and modulating the saturation of the color of the pixel in proportion to the 13. absolute value of the deviation of the background component from the reference value.

10. An apparatus as claimed in Claim 8 or 9, characterized in that the filter means comprises a two-dimensional homomorphic filter.

11. An apparatus as claimed in any one of Claims 8 - 10, characterized in that the means which produce the image signal comprises an echo-ultrasound scanner.

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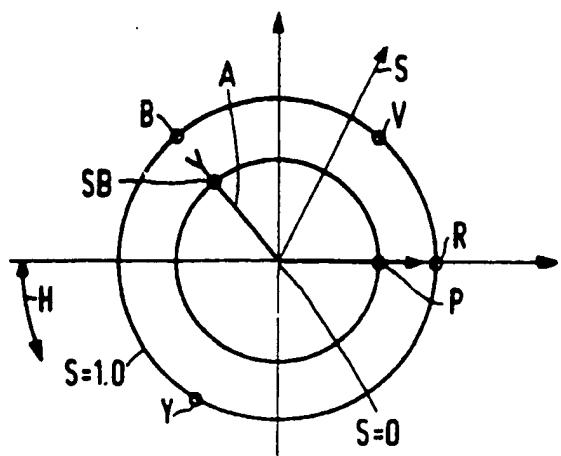


FIG.1

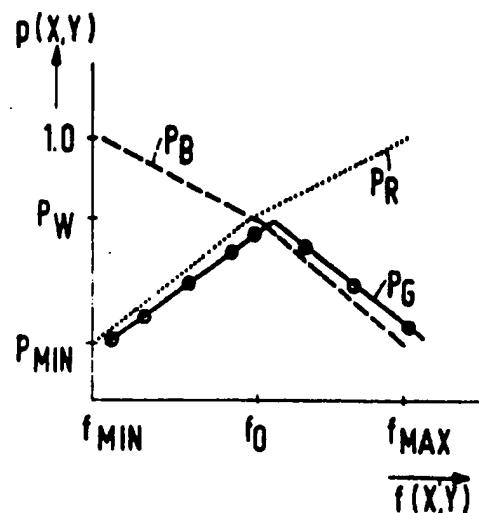


FIG.3

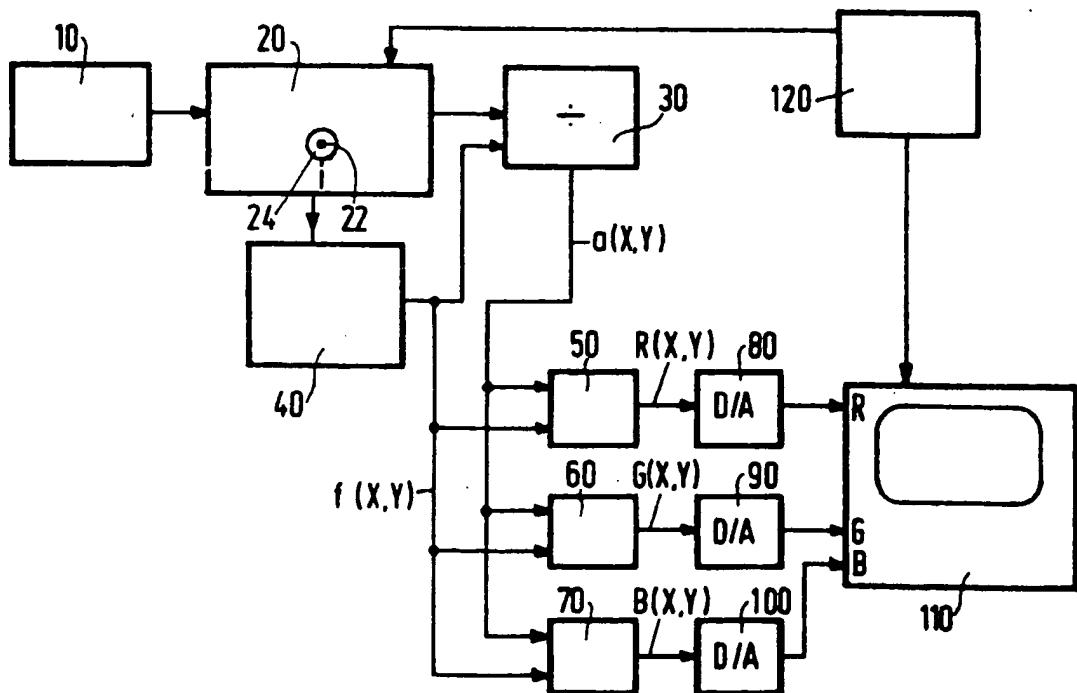


FIG.2



DOCUMENTS CONSIDERED TO BE RELEVANT		Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int. Cl.4)
Category	Citation of document with indication, where appropriate, of relevant passages		
Y	OPTICAL ENGINEERING, vol. 21, no. 1, January/February 1982, pages 108-112; Society of Photo-Optical Instrumentation Engineers; T. PELI et al.: "Adaptive filtering for image enhancement" * Whole document *	1-3, 8, 9	G 09 G 1/28 G 01 S 7/62 G 06 F 15/68
Y	US-A-4 007 327 (COUSIN) * Abstract; column 1, lines 6-8, 29-54; column 5, line 13 - column 8, line 23 *	1-3, 8, 9	
A	US-A-4 494 838 (WALLQUIST et al.) * Abstract; column 2, lines 38-62 *	1, 8	
A	EP-A-0 082 318 (HUGHES AIRCRAFT) * Abstract *	1, 8	G 09 G G 01 S G 06 F
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The present search report has been drawn up for all claims			
Place of search THE HAGUE	Date of compilation of the search 17-11-1986	Examiner OLDROYD D. L.	
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A	<p>IEEE TRANSACTIONS ON NUCLEAR SCIENCE, vol. NS-29, no. 4, August 1982, pages 1322-1330, IEEE, New York, US; S.M. PIZER et al.: "Concepts of the display of medical images"</p> <p>* Pages 1327-1330: Sections entitled: "Methods for increasing contrast sensitivity"; "Abstract"</p> <p>*</p> <p>---</p>	1	
A	<p>PROCEEDINGS OF THE IEEE, vol. 66, no. 12, December 1978, pages 1640-1651, IEEE, New York, US; W.F. SCHREIBER: "Image processing for quality improvement"</p> <p>* Abstract; pages 1644-1646: Section VI entitled "Homomorphic filtering" *</p> <p>---</p>	4	
A	<p>IEEE CONFERENCE ON PATTERN RECOGNITION AND IMAGE PROCESSING, Chicago, Illinois, US, 31st May - 2nd June 1978, pages 1-7, IEEE, New York, US; R.C. WAAG et al.: "Digital processing to enhance features of ultrasound images"</p> <p>---</p>		TECHNICAL FIELDS SEARCHED (Int. Cl.4)
A	<p>IEEE SPECTRUM, vol. 9, no. 7, July 1972, pages 20-32; H.C. ANDREWS et al.: "Image processing by digital computer"</p> <p>---</p> <p>---</p>	-/-	
The present search report has been drawn up for all claims			
Place of search	Date of completion of the search	Examiner	
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A	US-A-4 149 152 (RUSSO) -----		
TECHNICAL FIELDS SEARCHED (Int. Cl.)			
The present search report has been drawn up for all claims			
Place of search THE HAGUE	Date of completion of the search 17-11-1986	Examiner OLDROYD D.L.	
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